

Topics in Continuum Mechanics applied to Biology/2:
Blood flow

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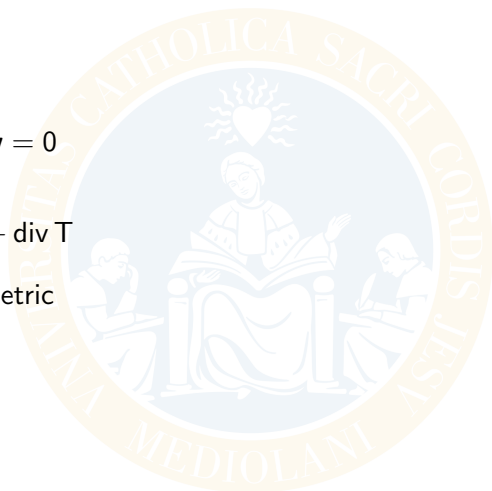
July 7, 2017

From the mathematical point of view (Eulerian)

$$\frac{d\rho}{dt} + \rho \operatorname{div} \mathbf{v} = 0 \quad (1)$$

$$\rho \frac{d\mathbf{v}}{dt} = \rho \mathbf{b} + \operatorname{div} \mathbf{T} \quad (2)$$

\mathbf{T} is symmetric (3)



We now have to make some assumptions on the form of T .



$$\mathbf{T} = -p\mathbf{I}$$

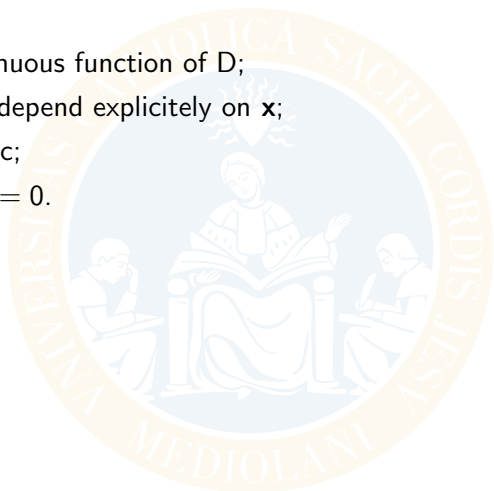


Stokesian fluids

“That the difference between the pressure on a plane in a given direction passing through any point P of a fluid in motion and the pressure which would exist in all directions about P if the fluid in its neighbourhood were in a state of relative equilibrium depends only on the relative motion of the fluid immediately about P ; and that the relative motion due to any motion of rotation may be eliminated without affecting the differences of the pressures above mentioned.” G.Stokes

Stokesian fluids

- V is a continuous function of D ;
- V does not depend explicitly on \mathbf{x} ;
- V is isotropic;
- $V = 0$, if $D = 0$.



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$$\mathbf{V} = \alpha \mathbf{I} + \beta D + \gamma D^2$$

But ...

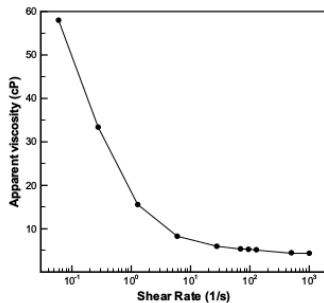
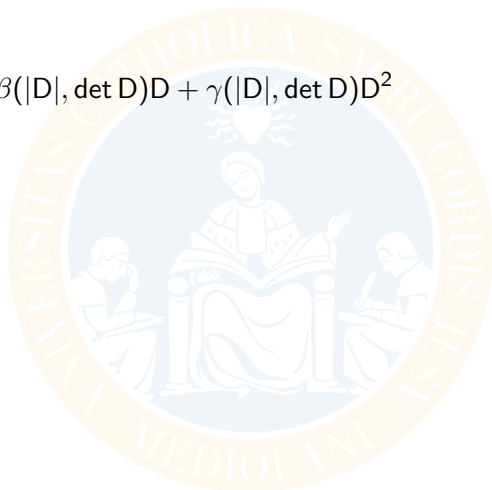


FIGURE 5. Apparent viscosity as a function of the shear rate for whole blood obtained from a 25 year old female donor with $Ht = 40\%$, $T = 23^\circ\text{C}$. Obtained using a Contraves LS30 (Couette) viscometer at shear rates of $\dot{\gamma} \in [0.06, 128] \text{ s}^{-1}$ and a Cannon–Manning Semi-Micro (capillary) viscometer, (Cannon Instrument Co.) at shear rates of $\dot{\gamma} \in [300, 1000] \text{ s}^{-1}$ (unpublished data from M. Kameneva, with permission).

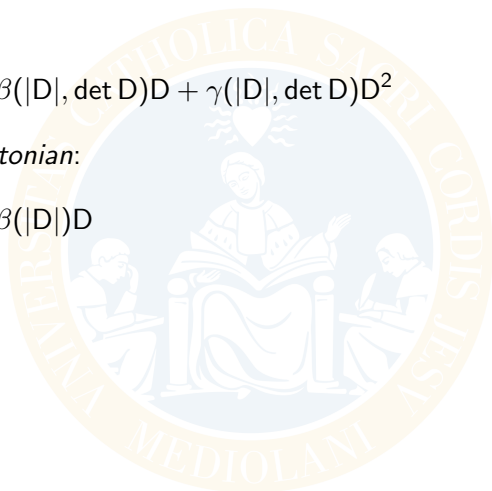
$$\mathbf{T} = -\tilde{p}\mathbf{I} + \beta(|\mathbf{D}|, \det \mathbf{D})\mathbf{D} + \gamma(|\mathbf{D}|, \det \mathbf{D})\mathbf{D}^2$$



$$\mathbf{T} = -\tilde{p}\mathbf{I} + \beta(|\mathbf{D}|, \det \mathbf{D})\mathbf{D} + \gamma(|\mathbf{D}|, \det \mathbf{D})\mathbf{D}^2$$

Generalized Newtonian:

$$\mathbf{T} = -\tilde{p}\mathbf{I} + \beta(|\mathbf{D}|)\mathbf{D}$$



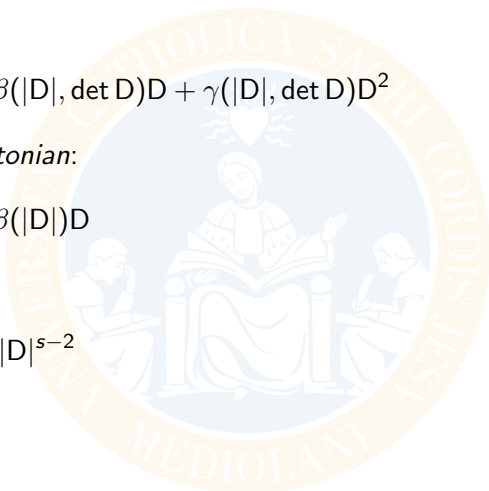
$$\mathbf{T} = -\tilde{p}\mathbf{I} + \beta(|\mathbf{D}|, \det \mathbf{D})\mathbf{D} + \gamma(|\mathbf{D}|, \det \mathbf{D})\mathbf{D}^2$$

Generalized Newtonian:

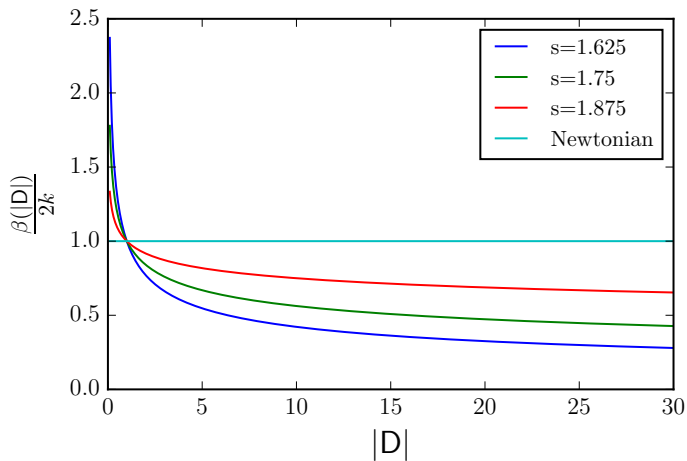
$$\mathbf{T} = -\tilde{p}\mathbf{I} + \beta(|\mathbf{D}|)\mathbf{D}$$

Power-law fluids:

$$\beta(|\mathbf{D}|) = 2k|\mathbf{D}|^{s-2}$$

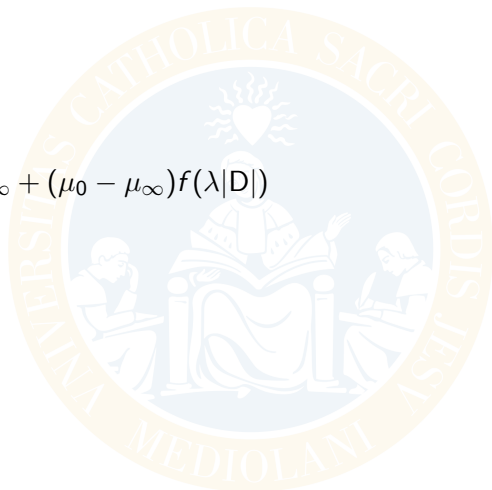


Power-law fluids



Non-Newtonian models

$$\beta(|D|) = \mu_{\infty} + (\mu_0 - \mu_{\infty})f(\lambda|D|)$$



Non-Newtonian models

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Model	Equation	Non-Newtonian Properties
Carreau-Yasuda	$\mu = \mu_{\infty} + \frac{\mu_0 - \mu_{\infty}}{[1 + (\lambda\dot{\gamma})^a]^{\frac{1-n}{a}}}$	shear thinning
Casson	$\tau^{1/2} = (k\dot{\gamma})^{1/2} + \tau_o^{1/2}$	yield stress
Power law	$\tau = k\dot{\gamma}^n$	shear thinning
Cross	$\mu = \mu_{\infty} + \frac{\mu_0 - \mu_{\infty}}{1 + \lambda\dot{\gamma}^m}$	shear thinning
Herschel-Bulkley	$\tau = k\dot{\gamma}^n + \tau_o$	shear thinning, yield stress
Oldroyd-B	$\tau + \lambda_1 \overset{\nabla}{\tau} = \mu_0 \left(\dot{\gamma} + \lambda_2 \overset{\nabla}{\dot{\gamma}} \right)$	viscoelasticity
Quemada	$\mu = \mu_p \left(1 - \frac{k_0 + k_{\infty} \sqrt{\dot{\gamma}/\dot{\gamma}_c}}{2(1 + \sqrt{\dot{\gamma}/\dot{\gamma}_c})} \phi \right)^{-2}$	shear thinning
Yelleswarapu	$\mu = \mu_{\infty} + (\mu_0 - \mu_{\infty}) \frac{1 + \ln(1 + \lambda\dot{\gamma})}{1 + \lambda\dot{\gamma}}$	shear thinning
Bingham	$\tau = k\dot{\gamma} + \tau_o$	yield stress
Eyring-Powell	$\mu = \mu_{\infty} + \frac{(\mu_0 - \mu_{\infty}) \sinh^{-1}(\lambda\dot{\gamma})}{\lambda\dot{\gamma}}$	shear thinning
Ree-Eyring	$\tau = \tau_c \sinh^{-1} \left(\frac{\mu_0 \dot{\gamma}}{\tau_c} \right)$	shear thinning

Non-Newtonian models

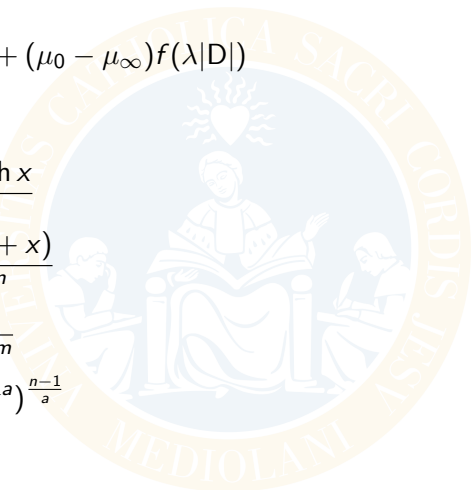
$$\beta(|D|) = \mu_\infty + (\mu_0 - \mu_\infty)f(\lambda|D|)$$

$$f(x) = \frac{\operatorname{arcsinh} x}{x}$$

$$f(x) = \frac{\log(1+x)}{x^m}$$

$$f(x) = \frac{1}{1+x^m}$$

$$f(x) = (1+x^a)^{\frac{n-1}{a}}$$



Non-Newtonian models

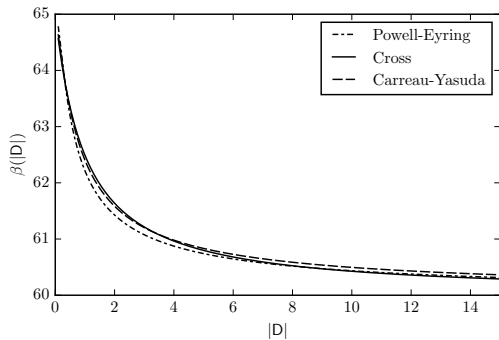
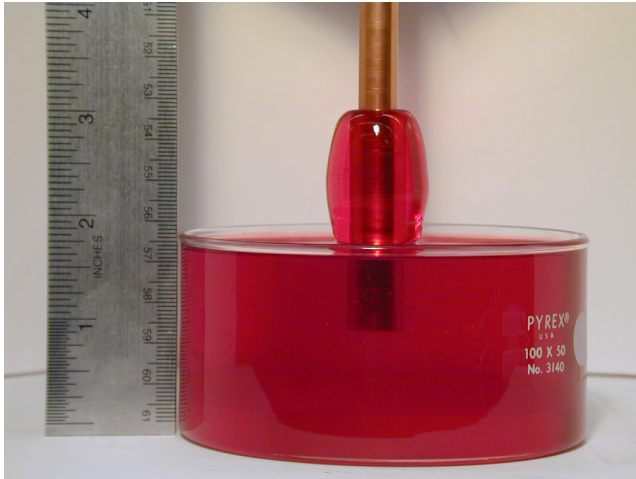


Figure: Un confronto fra i tre modelli newtoniani generalizzati principali per il sangue, con $\mu_0 = 65 \text{ kg m}^{-1} \text{ s}^{-1}$ e $\mu_\infty = 60 \text{ kg m}^{-1} \text{ s}^{-1}$. Inoltre, per il modello di Powell-Eyring si è scelto $\lambda = 5.383 \text{ s}$, per quello di Cross $\lambda = 1.007 \text{ s}$ e $m = 1.028$, per quello di Carreau-Yasuda $\lambda = 1.902 \text{ s}$, $n = 0.22$ e $a = 1.25$.

Rod climbing



$$\begin{aligned}
\nabla f &= \frac{\partial f}{\partial r} \mathbf{e}_r + \frac{1}{r} \frac{\partial f}{\partial \vartheta} \mathbf{e}_\vartheta + \frac{\partial f}{\partial z} \mathbf{e}_z, \\
\operatorname{div} \mathbf{u} &= \frac{1}{r} \frac{\partial(r u_r)}{\partial r} + \frac{1}{r} \frac{\partial u_\vartheta}{\partial \vartheta} + \frac{\partial u_z}{\partial z}, \\
\nabla \mathbf{u} &= \frac{\partial u_r}{\partial r} \mathbf{e}_r \otimes \mathbf{e}_r + \frac{\partial u_\vartheta}{\partial r} \mathbf{e}_\vartheta \otimes \mathbf{e}_r + \frac{1}{r} \left(\frac{\partial u_r}{\partial \vartheta} - u_\vartheta \right) \mathbf{e}_r \otimes \mathbf{e}_\vartheta + \frac{1}{r} \left(\frac{\partial u_\vartheta}{\partial \vartheta} + u_r \right) \mathbf{e}_\vartheta \otimes \mathbf{e}_\vartheta \\
&\quad + \frac{\partial u_r}{\partial z} \mathbf{e}_r \otimes \mathbf{e}_z + \frac{\partial u_\vartheta}{\partial z} \mathbf{e}_\vartheta \otimes \mathbf{e}_z + \frac{\partial u_z}{\partial z} \mathbf{e}_z \otimes \mathbf{e}_z + \frac{\partial u_z}{\partial r} \mathbf{e}_z \otimes \mathbf{e}_r + \frac{1}{r} \frac{\partial u_z}{\partial \vartheta} \mathbf{e}_z \otimes \mathbf{e}_\vartheta, \\
\Delta \mathbf{u} &= \left[\Delta u_r - \frac{1}{r^2} \left(u_r + 2 \frac{\partial u_\vartheta}{\partial \vartheta} \right) \right] \mathbf{e}_r + \left[\Delta u_\vartheta - \frac{1}{r^2} \left(u_\vartheta - 2 \frac{\partial u_r}{\partial \vartheta} \right) \right] \mathbf{e}_\vartheta + \Delta u_z \mathbf{e}_z, \\
\Delta f &= \frac{1}{r} \frac{\partial}{\partial r} \left(r \frac{\partial f}{\partial r} \right) + \frac{1}{r^2} \frac{\partial^2 f}{\partial \vartheta^2} + \frac{\partial^2 f}{\partial z^2}, \\
\operatorname{div} \mathbb{T} &= + \left[\frac{\partial \mathbb{T}_{rr}}{\partial r} + \frac{\mathbb{T}_{rr} - \mathbb{T}_{\vartheta\vartheta}}{r} + \frac{1}{r} \frac{\partial \mathbb{T}_{\vartheta r}}{\partial \vartheta} + \frac{\partial \mathbb{T}_{zr}}{\partial z} \right] \mathbf{e}_r + \\
&\quad + \left[\frac{\partial \mathbb{T}_{r\vartheta}}{\partial r} + \frac{2\mathbb{T}_{r\vartheta}}{r} + \frac{1}{r} \frac{\partial \mathbb{T}_{\vartheta\vartheta}}{\partial \vartheta} + \frac{\partial \mathbb{T}_{z\vartheta}}{\partial z} + \frac{\mathbb{T}_{\vartheta r} - \mathbb{T}_{r\vartheta}}{r} \right] \mathbf{e}_\vartheta + \\
&\quad + \left[\frac{\partial \mathbb{T}_{rz}}{\partial r} + \frac{\mathbb{T}_{rz}}{r} + \frac{1}{r} \frac{\partial \mathbb{T}_{\vartheta z}}{\partial \vartheta} + \frac{\partial \mathbb{T}_{zz}}{\partial z} \right] \mathbf{e}_z,
\end{aligned}$$